

Alignment and regularized reconstructions in tomography as optimization problems

IX Conferencia de Matemáticos Ecuatorianos en París

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Introduction, alignment in parallel tomography

example

Fan-beam tomography

alignment via fixed point iteration

Cone-beam tomography

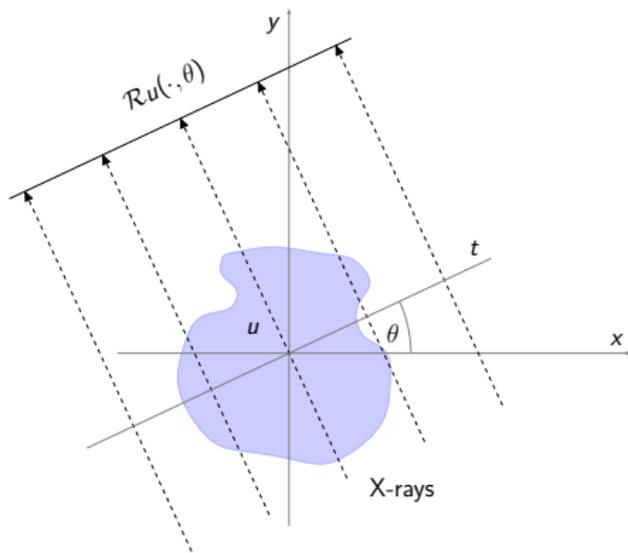
alignment via variable projection

on data

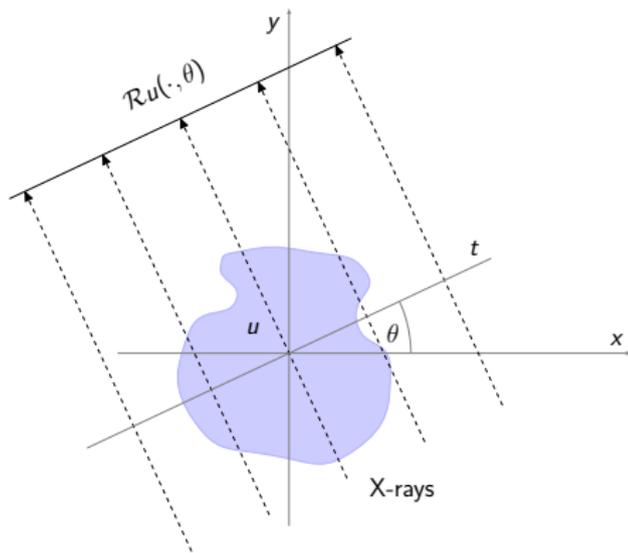
on real data

After alignment, regularized reconstruction

Conclusions and perspectives

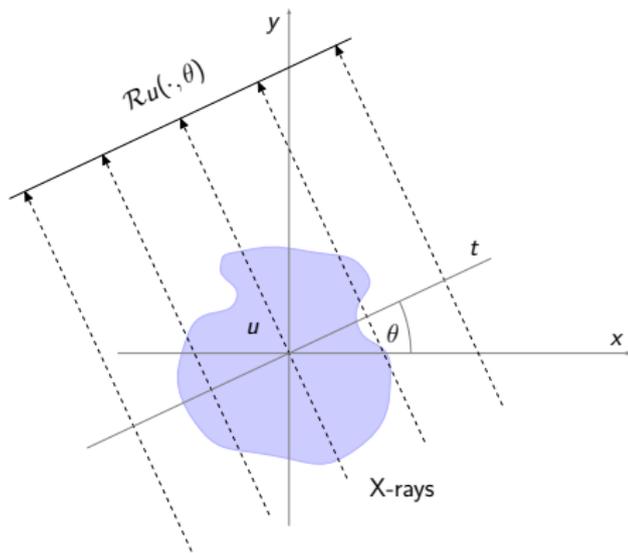


- u : object to be measured
- $v := \mathcal{R}u$: Radon transform of u : X-ray projections or sinogram

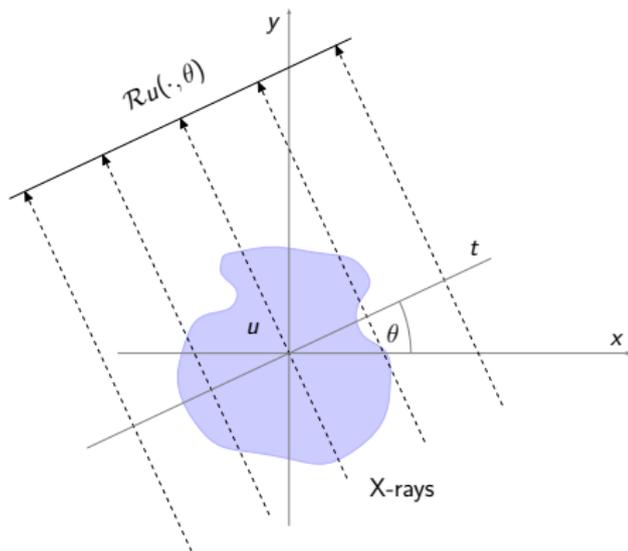


- Tomographic inverse problem:

given $v \in \mathfrak{R}(\mathcal{R})$, find $u \in U$ such that $\mathcal{R}u = v$



- What we measure: misaligned sinogram $\tilde{v}(t, \theta) = v(t-h, \theta)$, $h \in \mathbb{R}$



- What we measure: misaligned sinogram $\tilde{v}(t, \theta) = v(t-h, \theta)$, $h \in \mathbb{R}$
- Tomographic *alignment* inverse problem

given \tilde{v} , find $h \in \mathbb{R}$ such that $\tilde{v}(\cdot + h, \cdot) \in \mathfrak{A}(\mathcal{R})$

Introduction, alignment in parallel tomography example

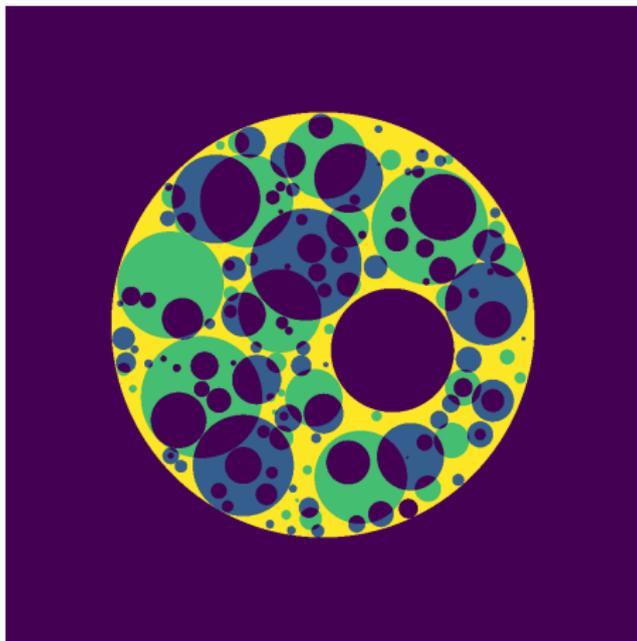
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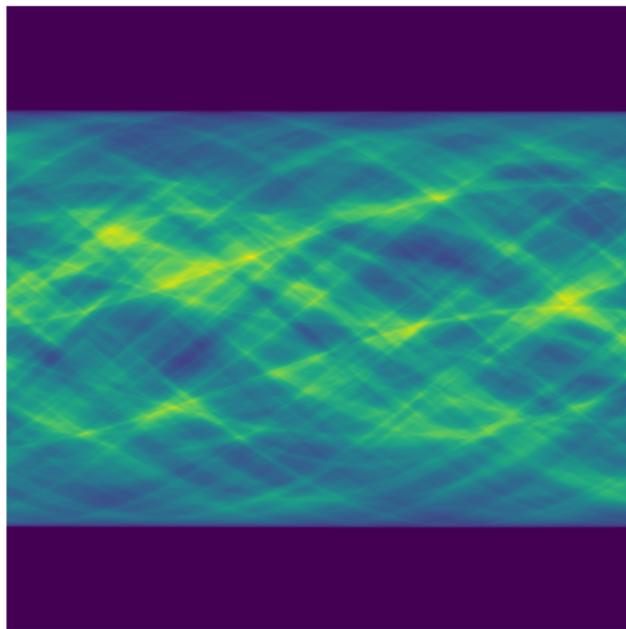
Conclusions and perspectives

- Numerical phantom¹

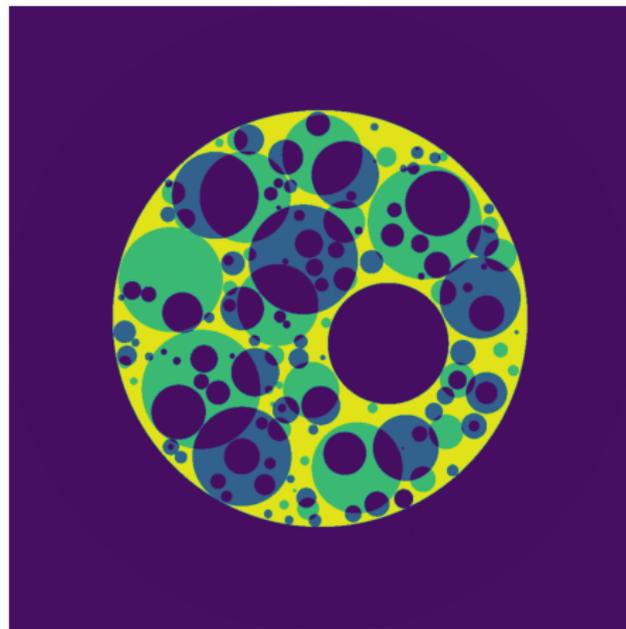


¹based on the `foam_ct_phantom` library

- Conventional (FBP) reconstruction²



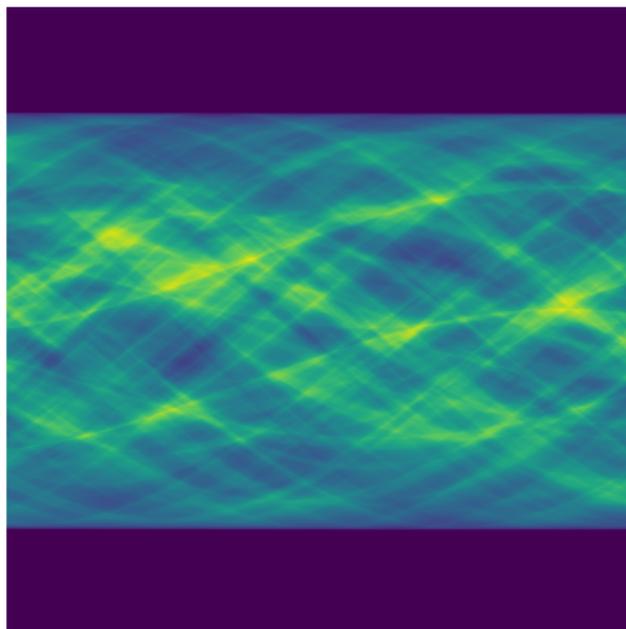
$\theta \in [0, \pi[$
 $\mathcal{R}f$ (sinogram)



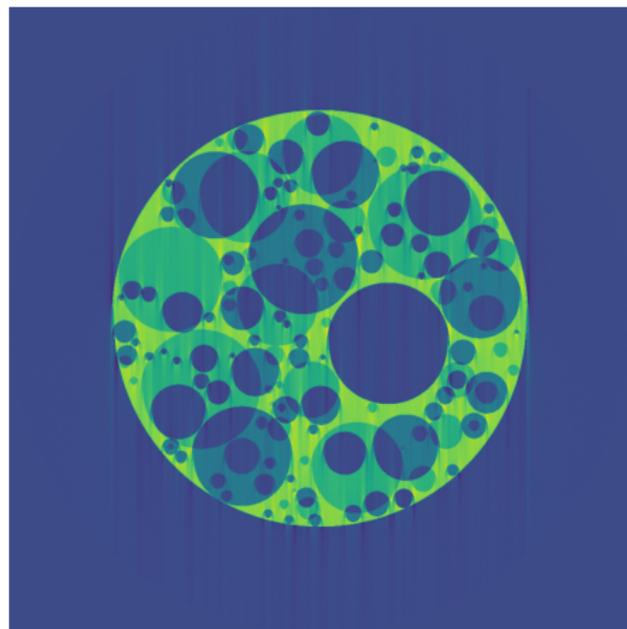
FBP reconstruction

²Kak, Slaney. 1988

- Conventional (FBP) reconstruction



$\theta \in [0, \pi[$
 $\mathcal{R}f, h = 2$ pixels



FBP reconstruction

- **Parity:** alignment for parallel projections, based on

$$v(t, \theta) = v(-t, \theta + \pi), \quad \forall (t, \theta)$$

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- We know

$$\tilde{v}(t + h, \theta) = \tilde{v}(-t + h, \theta + \pi), \quad \forall (t, \theta)$$

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- With $q = t + h$

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- Then, h is found with 1D signal registration:

$$h^* = \frac{1}{2} \text{shift}(\tilde{v}(\cdot, 0), \tilde{v}(-\cdot, \pi)) = \frac{1}{2} \operatorname{argmax}_{t \in \mathbb{R}} \tilde{v}(\cdot, 0) \star \tilde{v}(-\cdot, \pi)$$

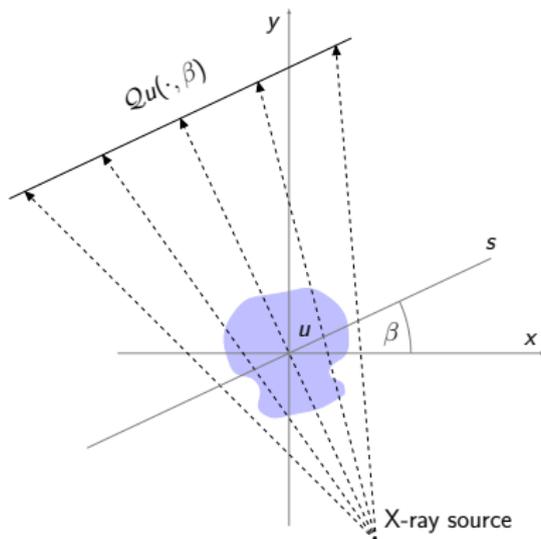
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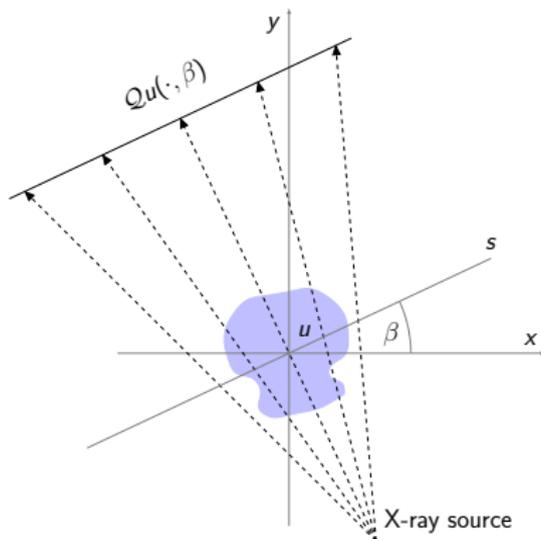
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Conclusions and perspectives

- Fan-beam symmetry:

$$v(s, \beta) = v(-s, \beta + 2 \arctan \frac{s}{r} + \pi), \quad \forall (s, \beta)$$

r : source-object distance, or source radius

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- We have now

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- with $q = s + h$

$$\tilde{v}(q, 0) = \tilde{v}(-q + 2h, 2 \arctan \frac{q - h}{r} + \pi), \quad \forall q \quad (1)$$

- Denote the operators

$$\begin{cases} \Lambda v(q) = v(q, 0) \\ \Pi_h v(q) = v(-q + 2h, 2 \arctan \frac{q-h}{r} + \pi) \end{cases}$$

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- and find h^* by solving

$$\min_h \{L(h) := \|\Lambda \tilde{g} - \Pi_h \tilde{g}\|_2^2\}$$

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- L differentiable, locally convex, any gradient based algorithm works :

$$h_{k+1} = h_k - \gamma_k \frac{d}{dh} L(h)$$

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- Works on real fan-beam data: < 20 iterations

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Lemma (arxiv:2310.09567, 2023)

\tilde{v} verifies

$$\Lambda \tilde{v}(q) \approx \Pi_0 \tilde{v}(q - 2h^*), \quad \forall q \in \mathbb{R}$$

with an error bounded by

$$\max_q |\Lambda \tilde{v}(q) - \Pi_0 \tilde{v}(q - 2h^*)| \leq C_{h^*},$$

with

$$C_{h^*} = \max_{q, \beta} \left| \tilde{v}(q, \beta) - \tilde{v}(q, \beta + \frac{2h^*}{r}) \right|$$

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$$h^* \approx \frac{1}{2} \text{shift}(\Lambda \tilde{v}, \Pi_0 \tilde{v})$$

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$$T_{\tilde{v}}(h) = h + \frac{1}{2} \text{shift}(\Lambda v, \Pi_h v)$$

- From (1), we have

$$\text{shift}(\Lambda \tilde{v}, \Pi_{h^*} \tilde{v}) = 0$$

thus h^* is a solution of

$$T_{\tilde{v}}(h) = h$$

i.e., h^* is a **fixed point** of $T_{\tilde{v}}$

Theorem (arxiv:2310.09567, 2023)

If the error C_{h^} is such that $T_{\tilde{v}}$ is a contraction in a neighbourhood of h^* . The fanbeam alignment problem has a unique solution as the limit of the iteration*

$$h_0 = 0, \quad h_{k+1} = T_{\tilde{v}}(h_k)$$

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- 2D interpolations required only in

$$\Pi_{h_k} \tilde{v} = \tilde{v}(-q + 2h_k, 2 \arctan \frac{q - h_k}{r} + \pi)$$

- Works on real fan-beam data: < 5 iterations

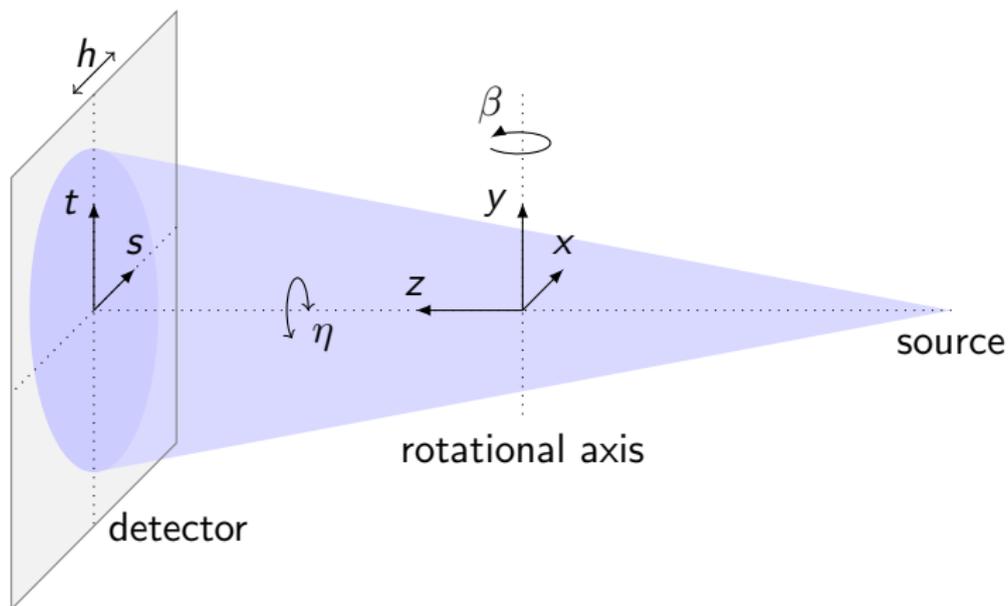
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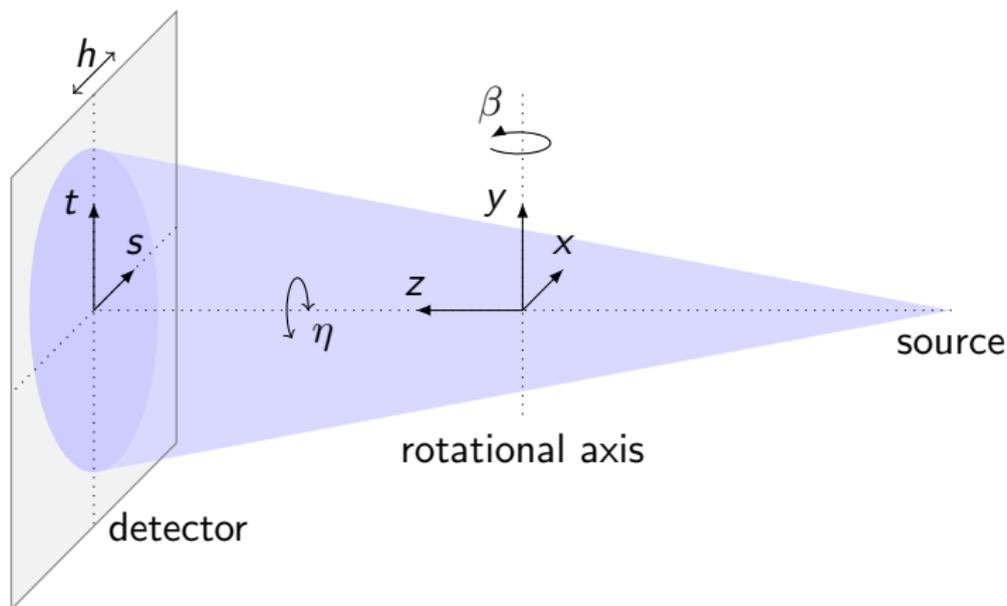
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Conclusions and perspectives



- $v := Cu$: Cone-beam transform of u parameterized with (s, t, β)



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- Alignment variables to estimate: $\{h, \eta\}$

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- **Notations:** Translation and rotation operators τ_h, κ_η :

$$\begin{cases} \tau_h v(s, t, \beta) = v(s - h, v, \beta) \\ \kappa_\eta v(u, v, \beta) = v(s \cos \eta - t \sin \eta, s \sin \eta + t \cos \eta, \beta) \end{cases}$$

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- We measure now :

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$$v(s, 0, \beta) = v(-s, 0, \beta + 2 \arctan \frac{s}{r} + \pi), \quad \forall (s, \beta)$$

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- It is clear that $\kappa_\eta^{-1} \tau_h^{-1} \tilde{v} = \kappa_{-\eta} \tau_{-h} \tilde{v} = v$ then we have

$$\kappa_{-\eta} \tau_{-h} \tilde{v}(s, 0, \beta) = \kappa_{-\eta} \tau_{-h} \tilde{v}(-s, 0, \beta + 2 \arctan \frac{s}{r} + \pi) \quad (2)$$

- Denote the operators

$$\begin{cases} \Lambda_{h,\eta} v(s, \beta) := \kappa_{-\eta} \tau_{-h} v(s, 0, \beta) \\ \Pi_{h,\eta} v(s, \beta) := \kappa_{-\eta} \tau_{-h} v(-s, 0, \beta + 2 \arctan \frac{s}{r} + \pi) \end{cases}$$

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- then (h^*, η^*) can be estimated by solving :

$$\min_{h,\eta} \{L(h, \eta) := \|\Lambda_{h,\eta} \tilde{v} - \Pi_{h,\eta} \tilde{v}\|_2^2\}$$

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- Too slow with standard quasi-newton methods

- Variable projection (VP) approach³

³Golub, Pereyra. SIAM J. Num. Analysis. 1973

- Variable projection (VP) approach³
- Project h onto η :

$$h^*(\eta) = \underset{h}{\operatorname{argmin}} L(h, \eta)$$

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with a *tilted* fanbeam fixed point approach **FP** previously introduced

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with a *tilted* fanbeam fixed point approach **FP** previously introduced

- and finally solve

$$\eta^* = \underset{\eta}{\operatorname{argmin}} \{ \bar{L}(\eta) := \|\Lambda_{h^*(\eta), \eta} \tilde{v} - \Pi_{h^*(\eta), \eta} \tilde{v}\|_2^2 \}$$

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Theorem (Aravkin, van Leeuwen. 2012)

If L twice-differentiable and locally convex then:

$$\frac{d}{d\eta} \bar{L}(\eta) = \nabla_{\eta} L(h^*(\eta), \eta)$$

and a local minimum η^ of \bar{L} with $h^*(\eta^*)$ is a local minimum of L*

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- The algorithm⁴:

$$\begin{cases} h_k = \mathbf{FP}(\eta_k) \\ \eta_{k+1} = \eta_k - \gamma_k \nabla_{\eta} L(h_k, \eta_k) \end{cases}$$

⁴arxiv:2310.09567, 2023

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- Depends on data, but works in < 5 minutes for 2000³ CT data with CPU python code and the Armijo step size rule⁵ for γ_k

⁴arxiv:2310.09567, 2023

⁵Nocedal, Wright. 2006

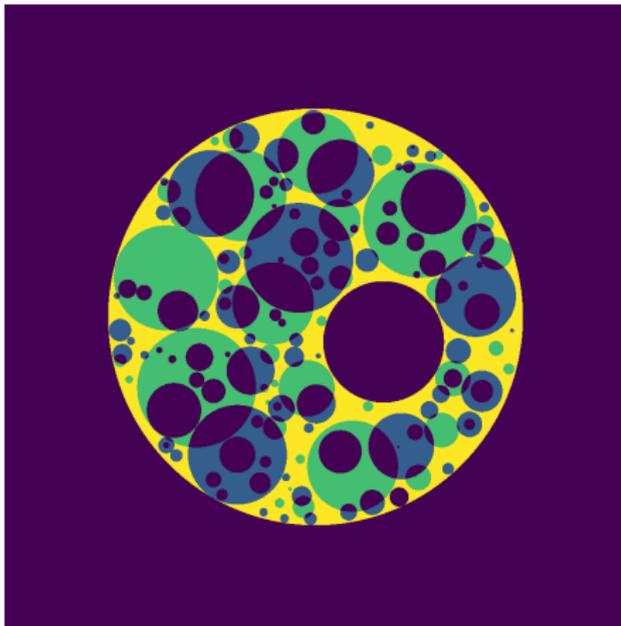
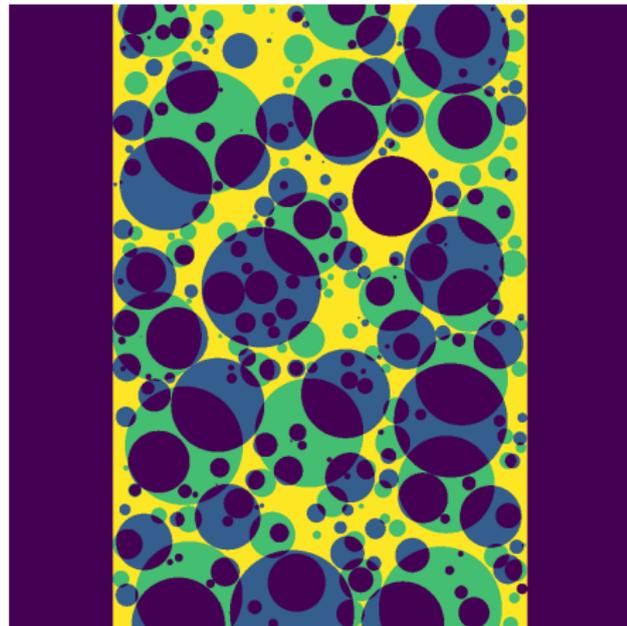
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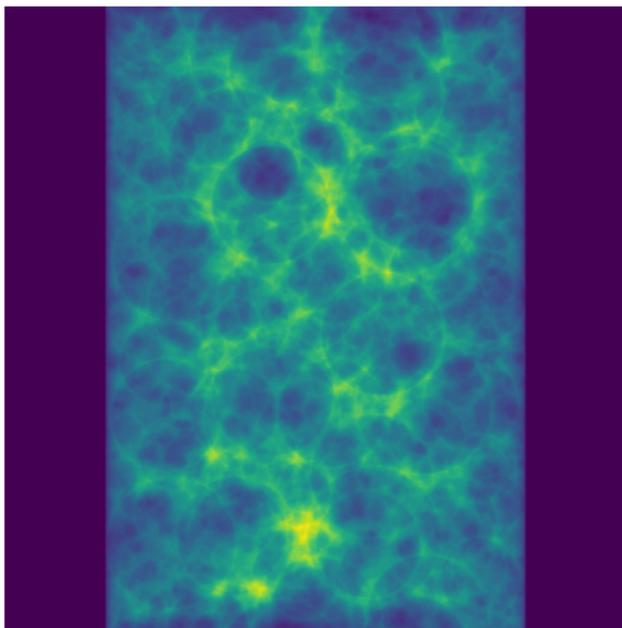
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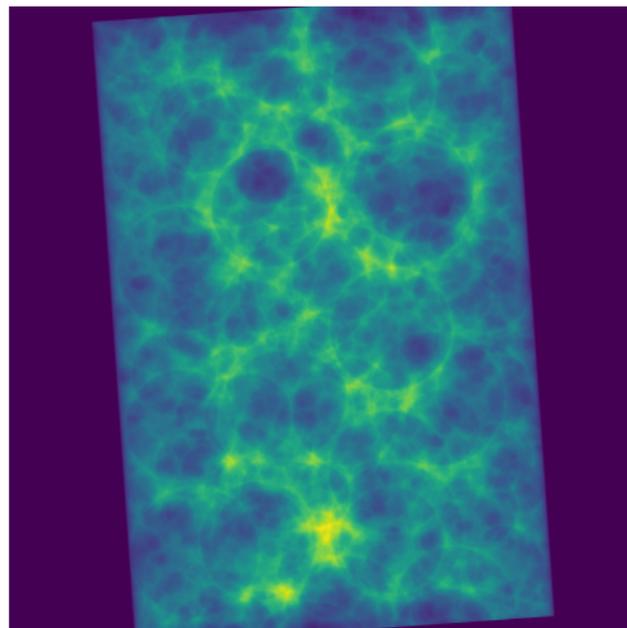
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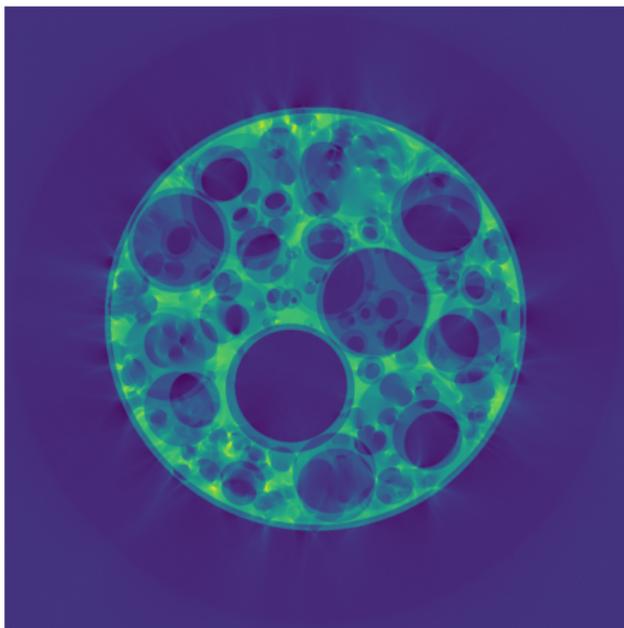
slice ($y = 0$)parallel to detector ($z = 0$)



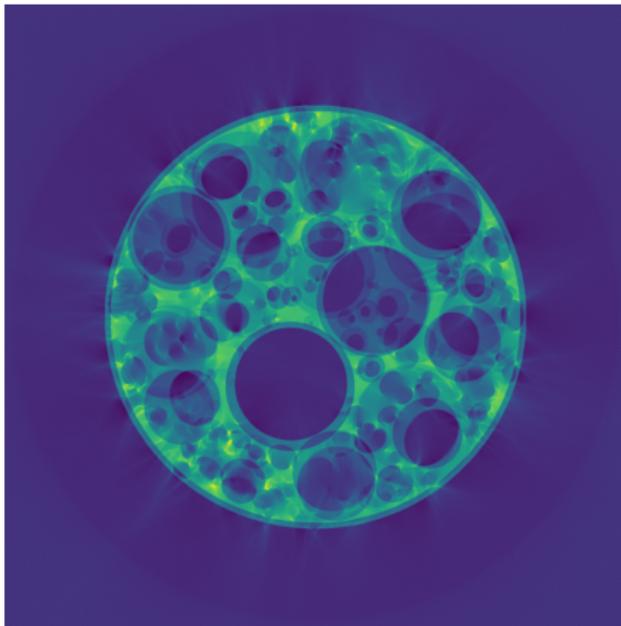
ideal conebeam projection



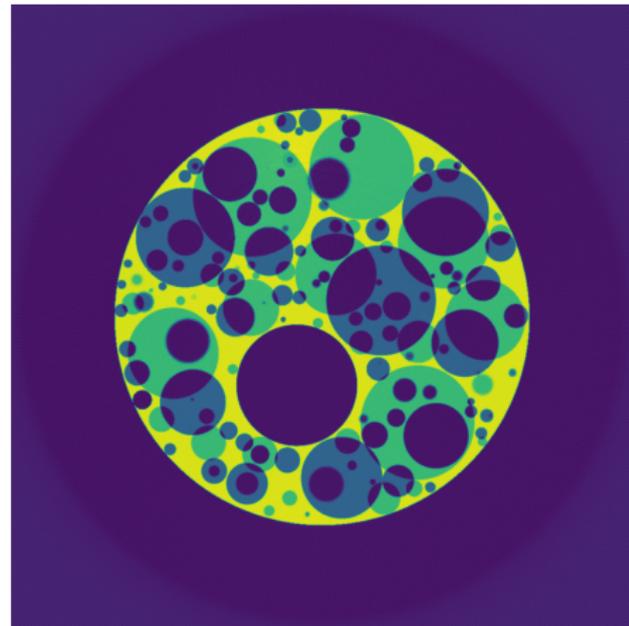
misaligned, $h = 5$ pix, $\eta = 4^\circ$



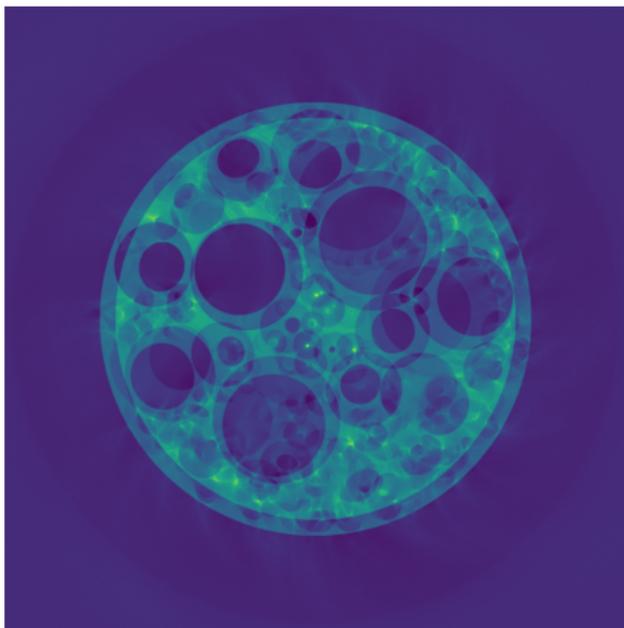
raw middle slice



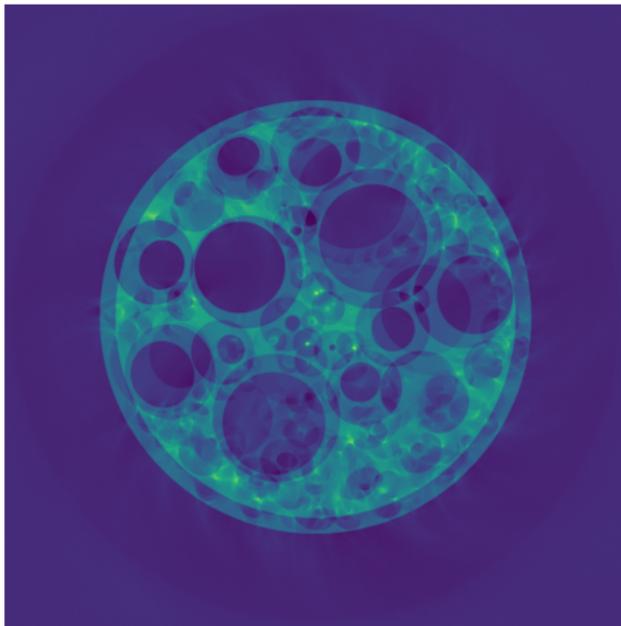
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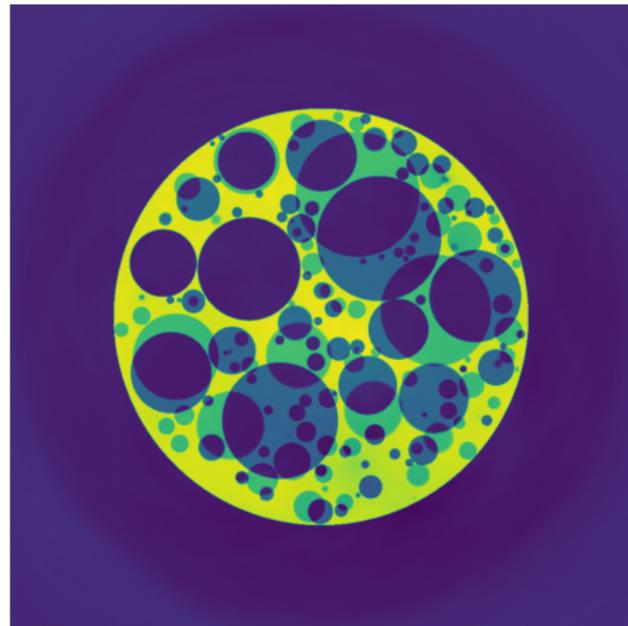
VP aligned middle slice



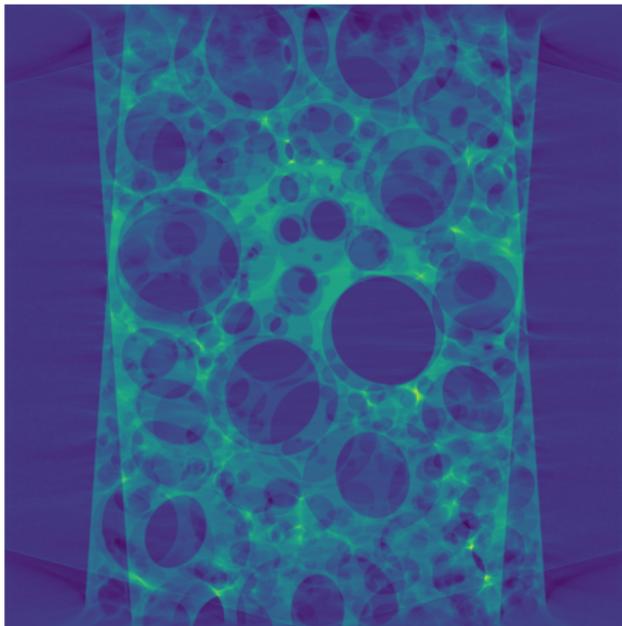
raw $\frac{1}{4}$ slice



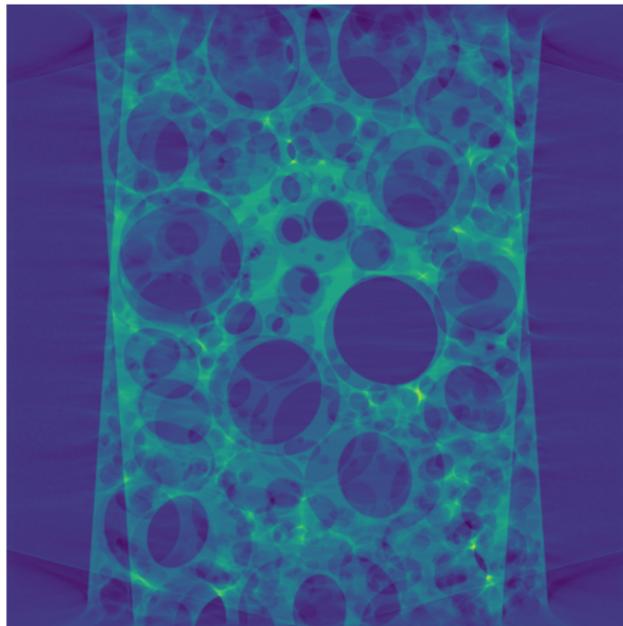
raw $\frac{1}{4}$ slice



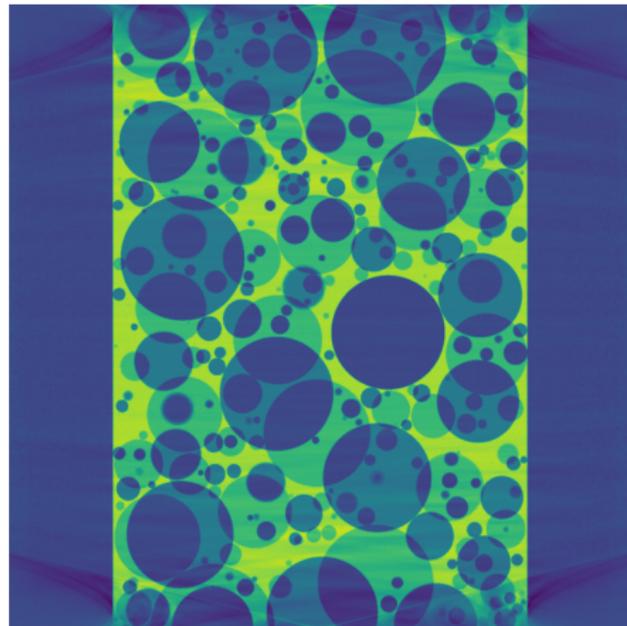
VP aligned $\frac{1}{4}$ slice



raw $z = 0$ slice



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VP aligned $z = 0$ slice

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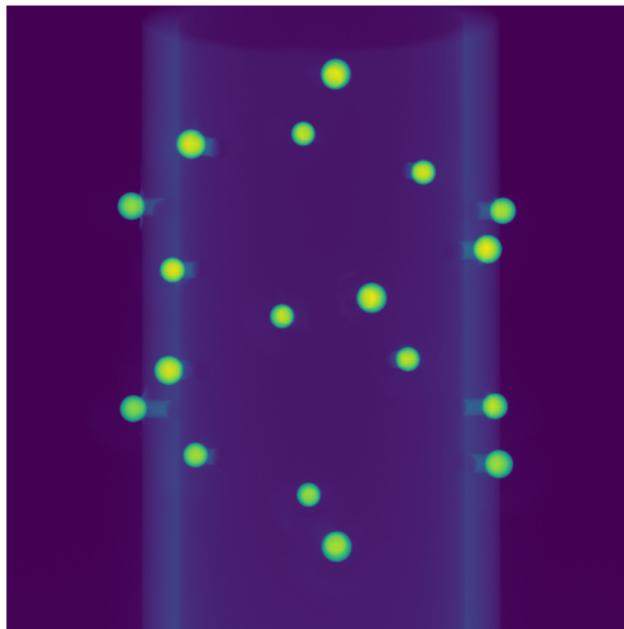
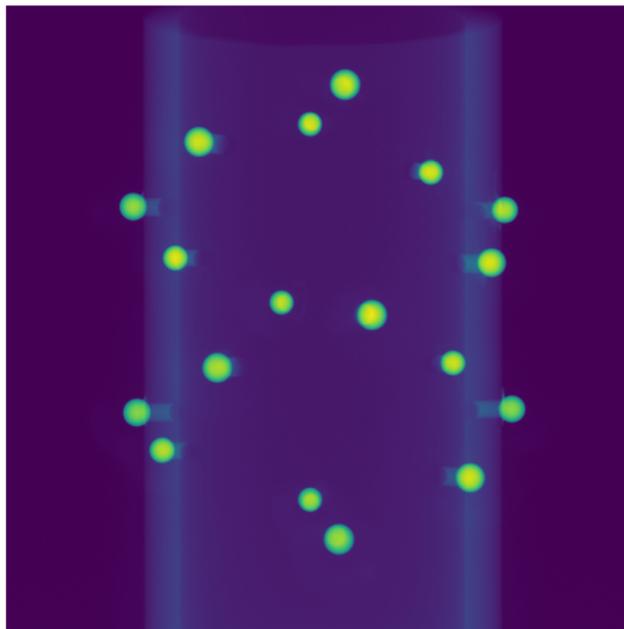
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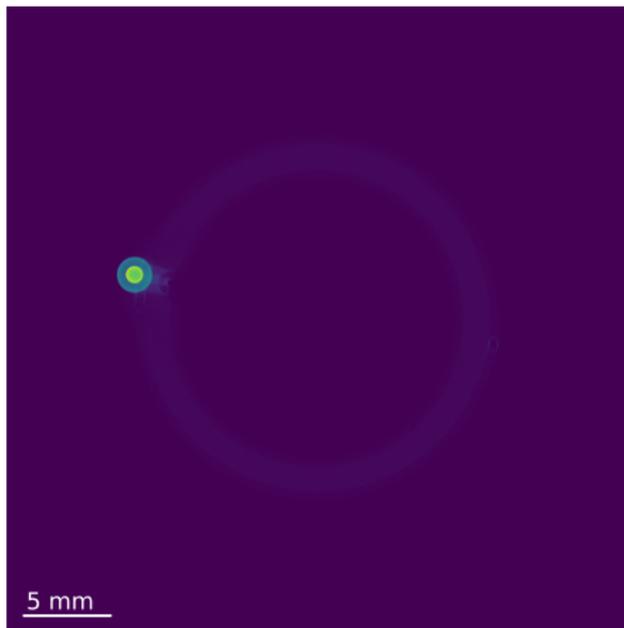
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Conclusions and perspectives

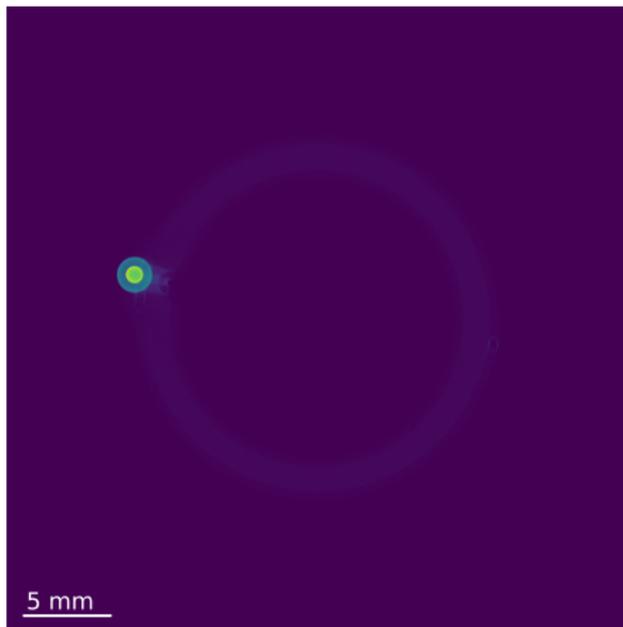
- Calibration object⁶

 $\beta = 0$  $\beta = \pi$

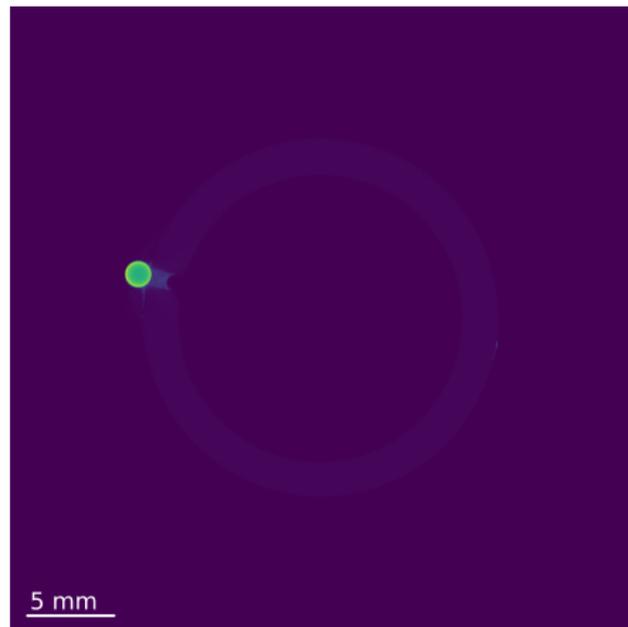
⁶M. Ferucci et al, Prec. Eng. 2021



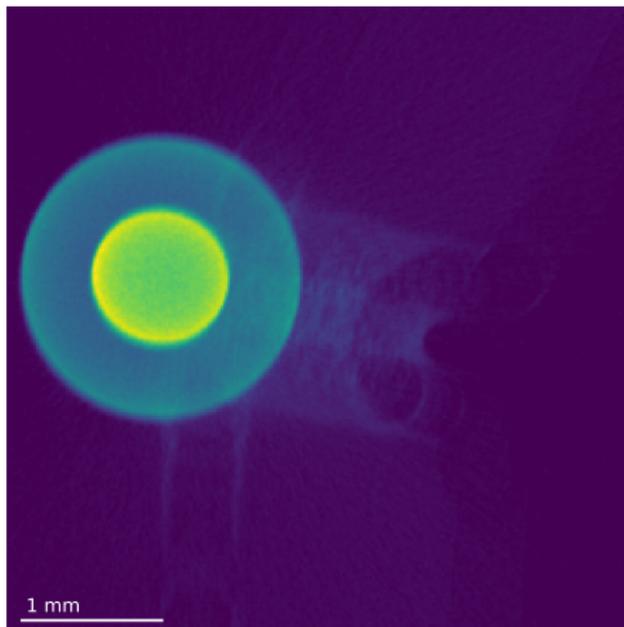
raw middle slice



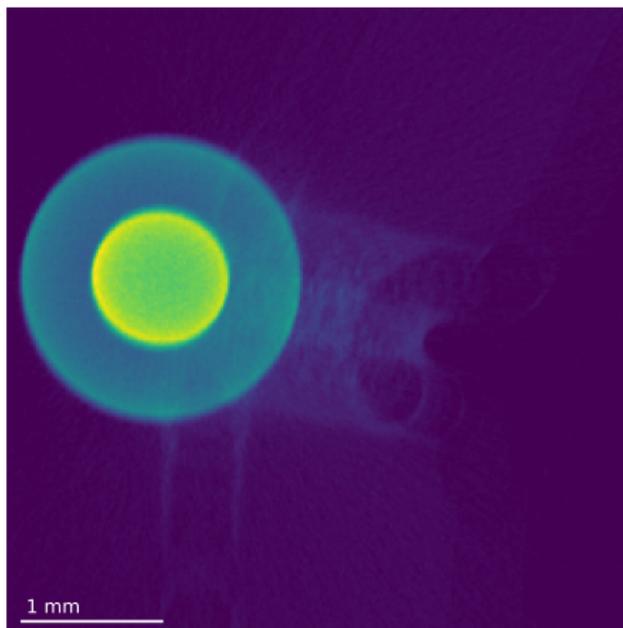
raw middle slice



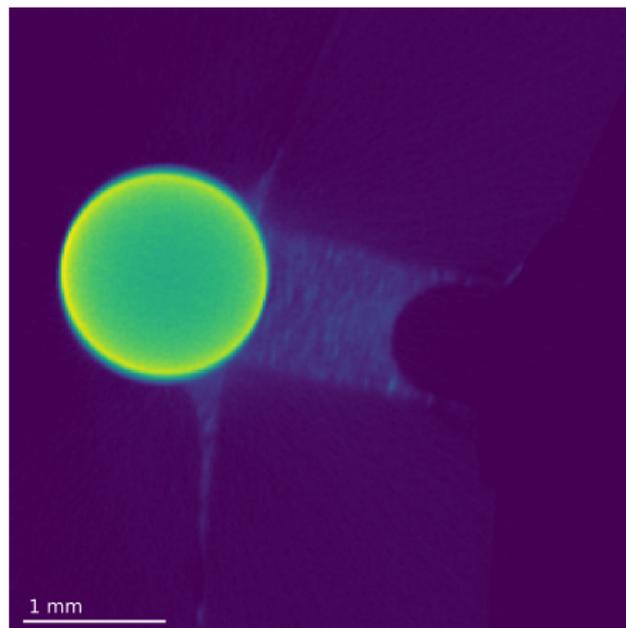
VP aligned



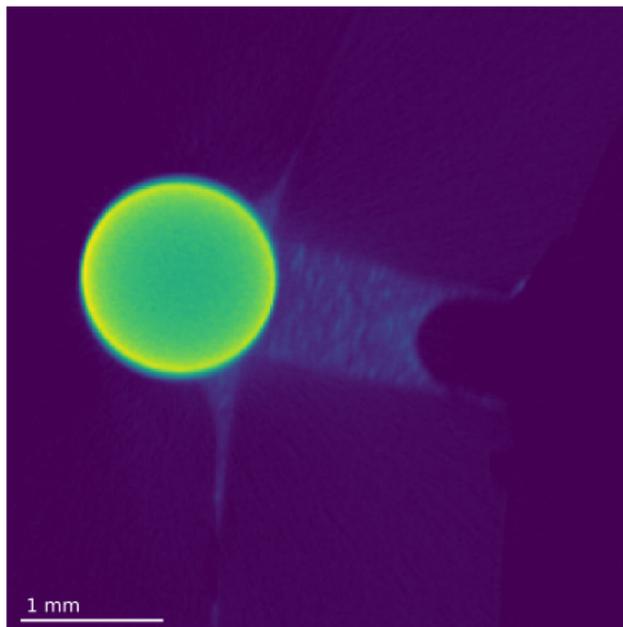
raw middle slice



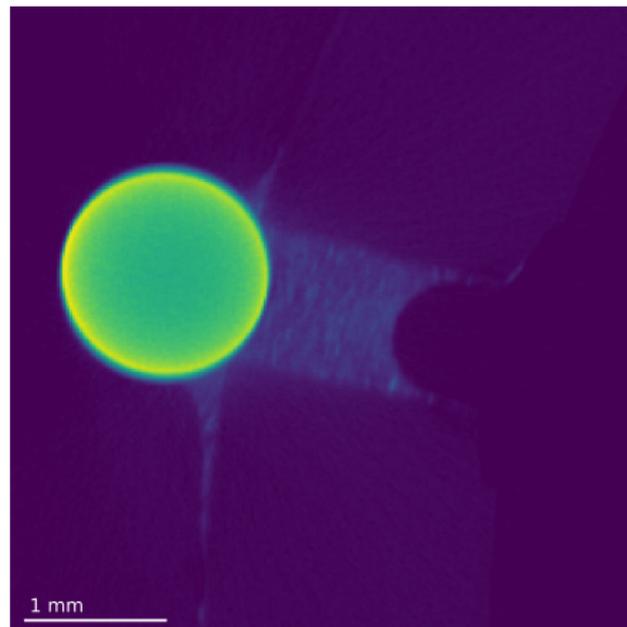
raw middle slice



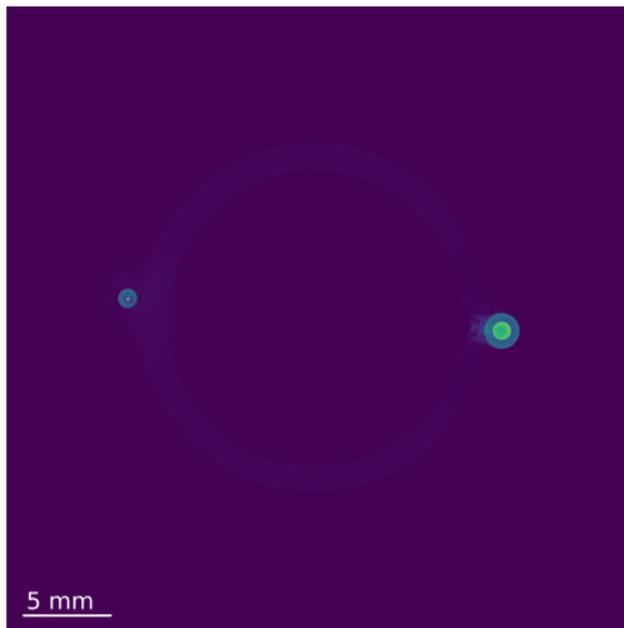
VP aligned



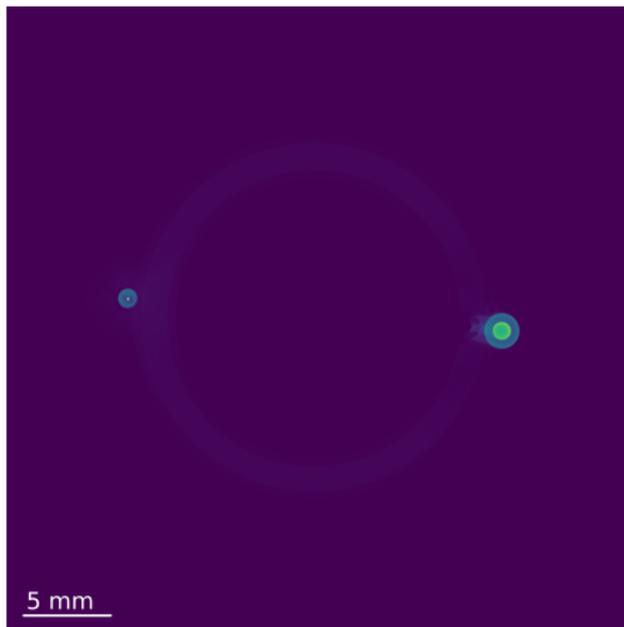
Reference-based method



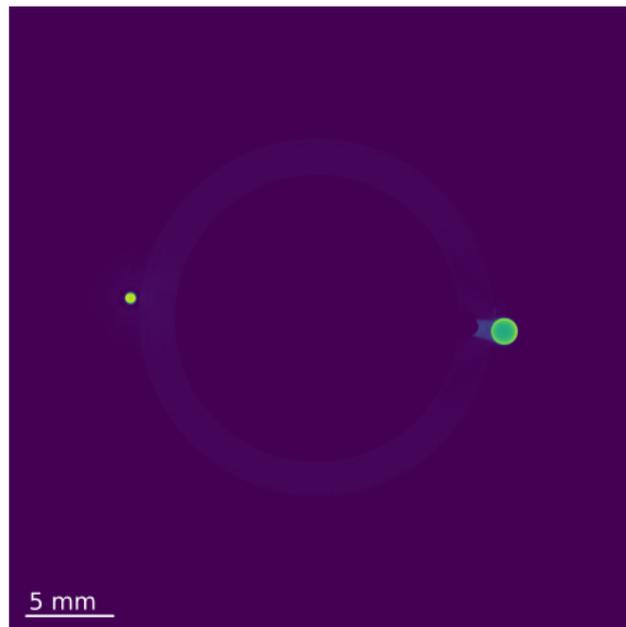
VP aligned



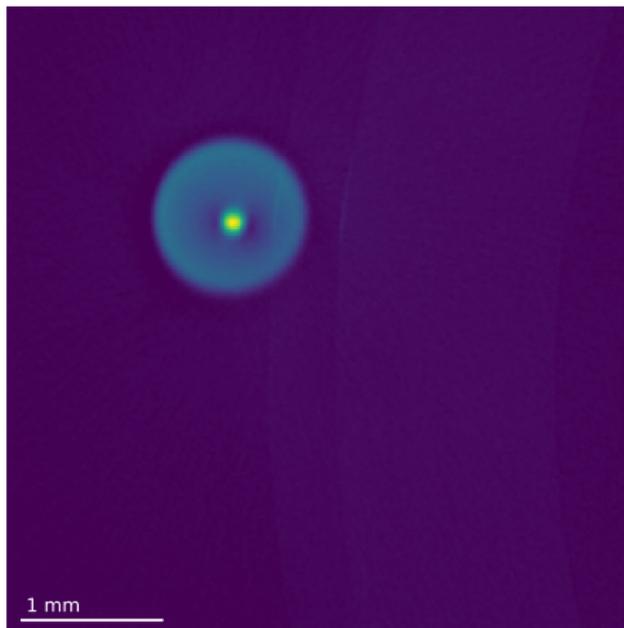
raw $\frac{1}{4}$ slice



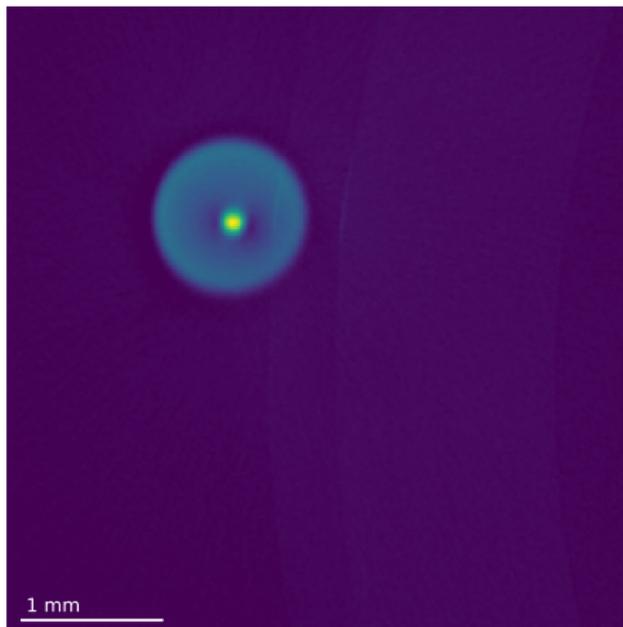
raw $\frac{1}{4}$ slice



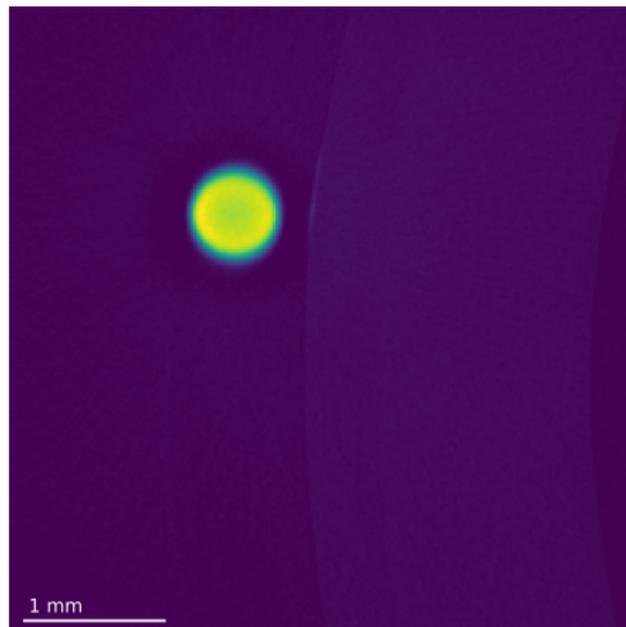
VP aligned



raw $\frac{1}{4}$ slice

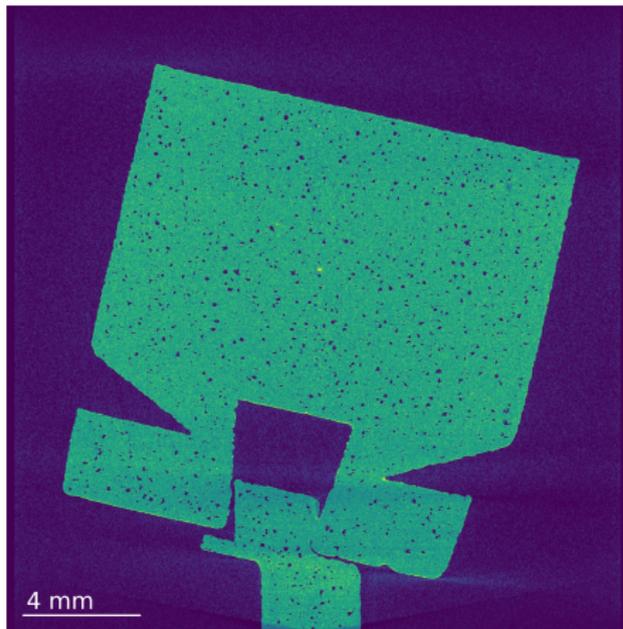


raw $\frac{1}{4}$ slice

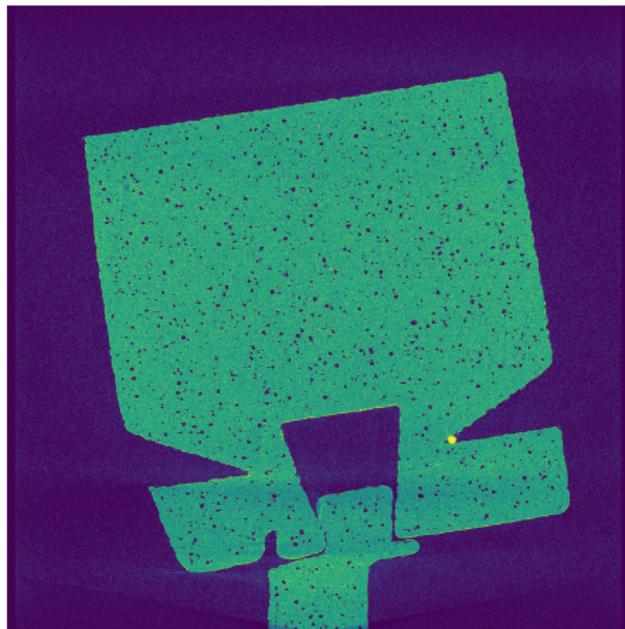


VP aligned

- Additive manufactured sample⁷



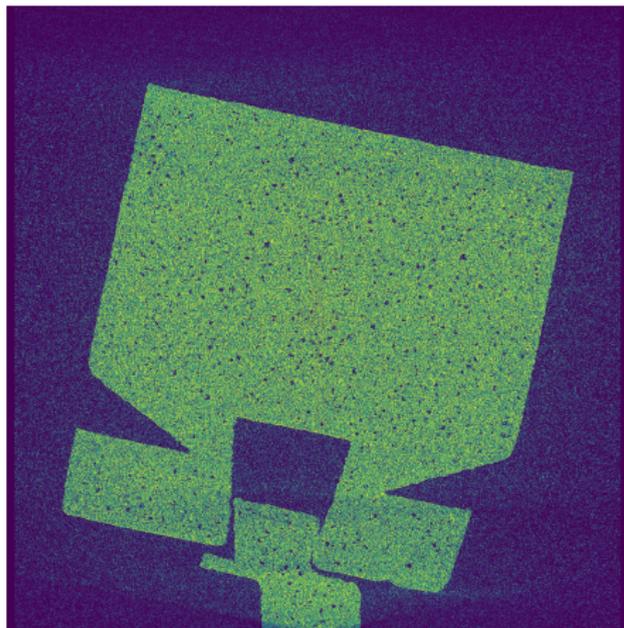
$z = 0$, VP aligned



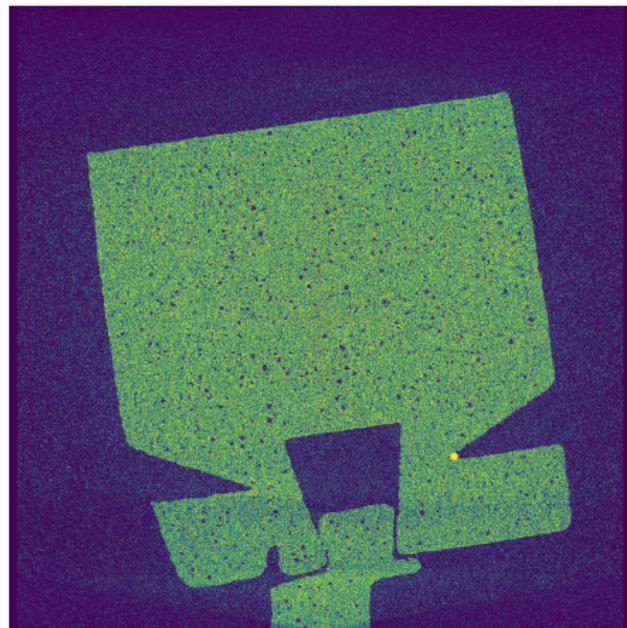
$y = 0$, VP aligned

⁷printed by R. Santander, KU Leuven

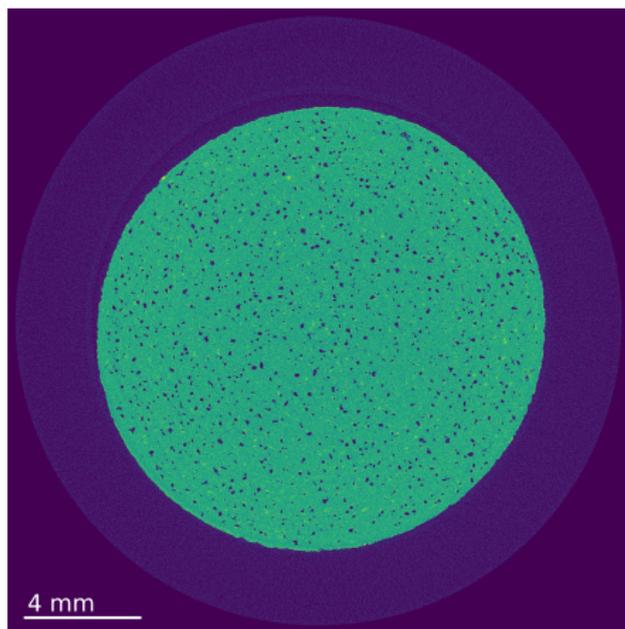
- Low quality (LQ) 5 min CT scan - high noise level



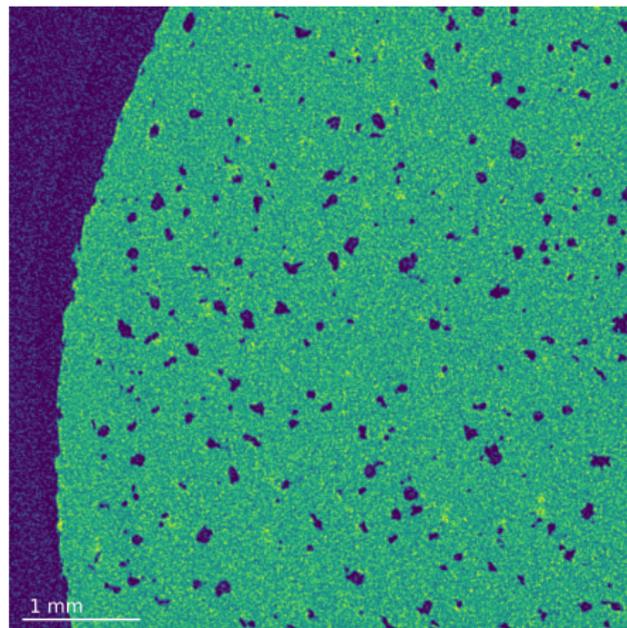
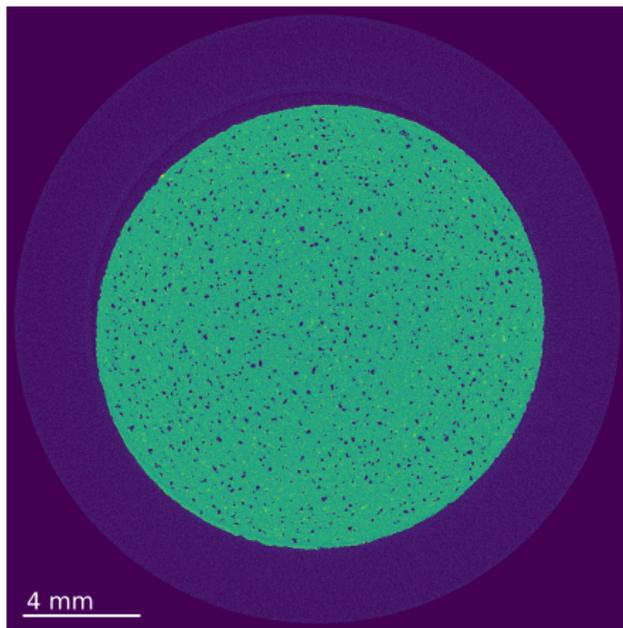
$z = 0$, VP aligned



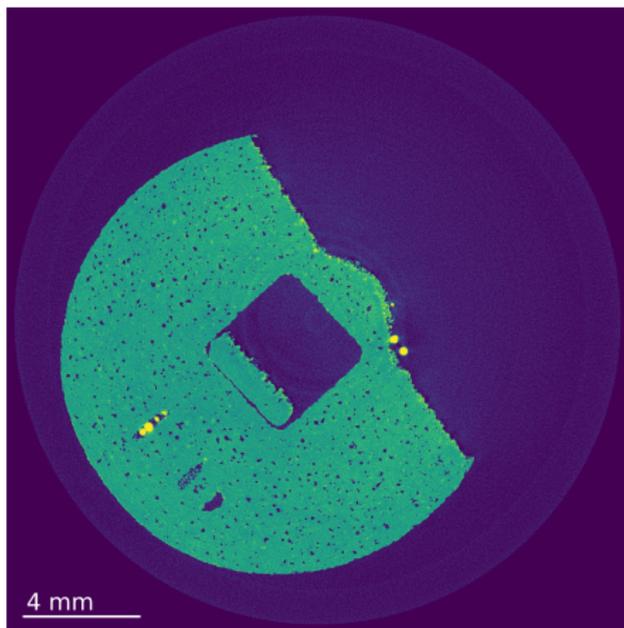
$y = 0$, VP aligned



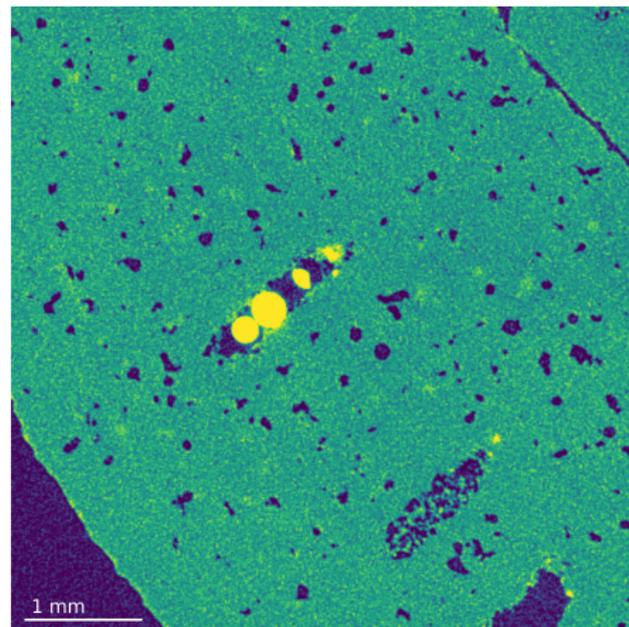
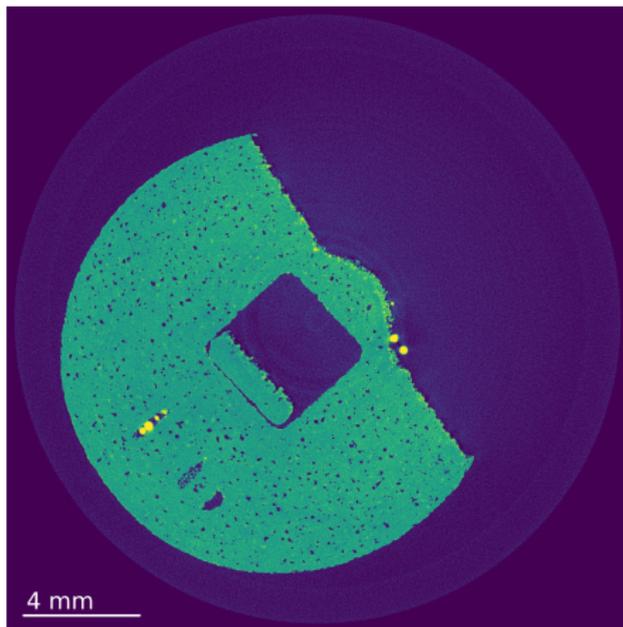
middle slice



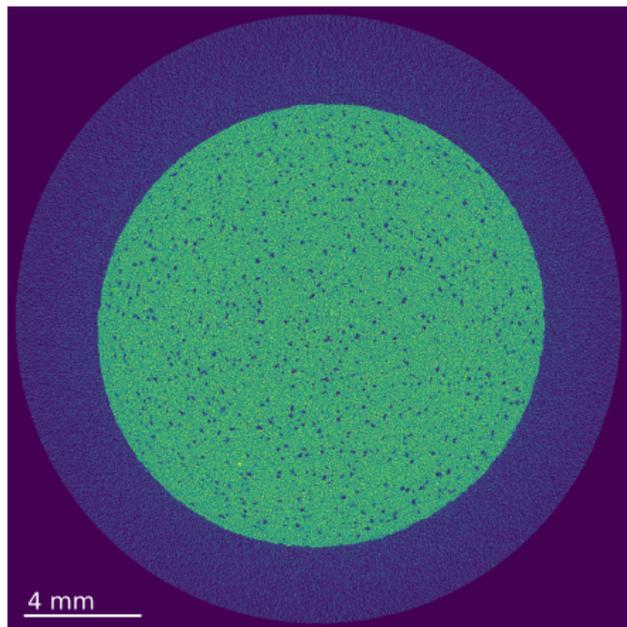
middle slice



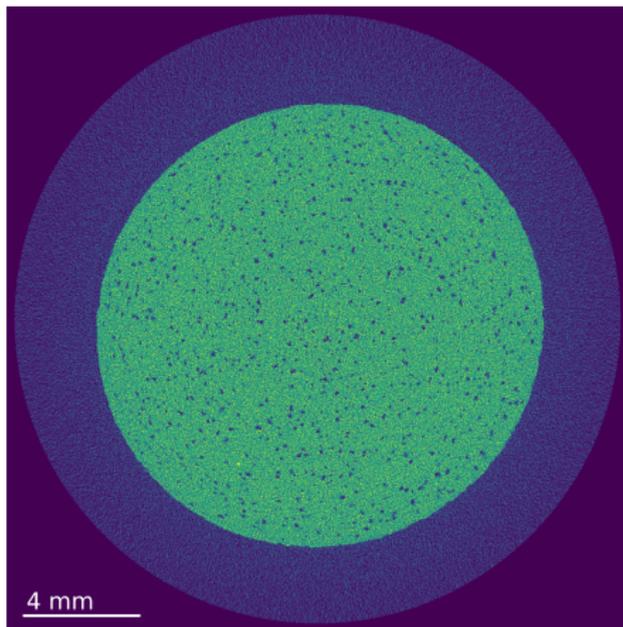
$\frac{1}{4}$ slice



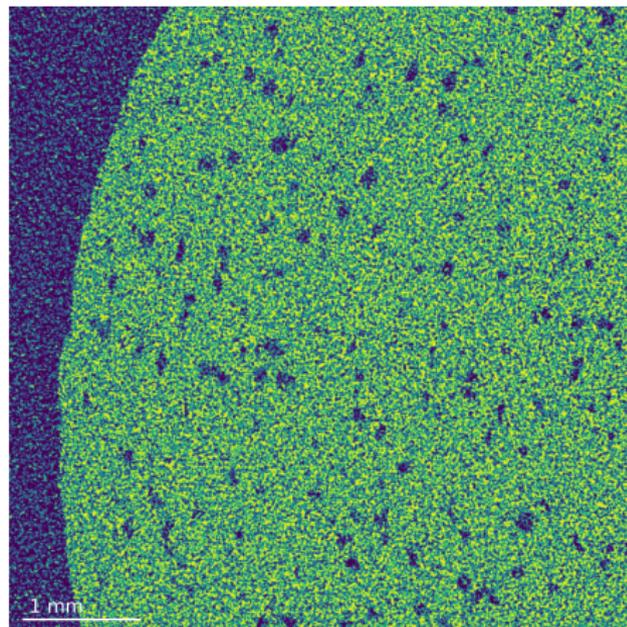
$\frac{1}{4}$ slice

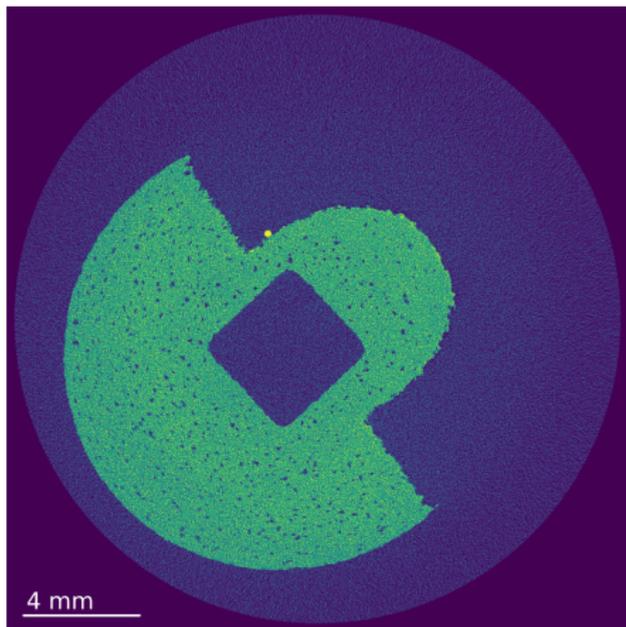


middle slice, LQ scan

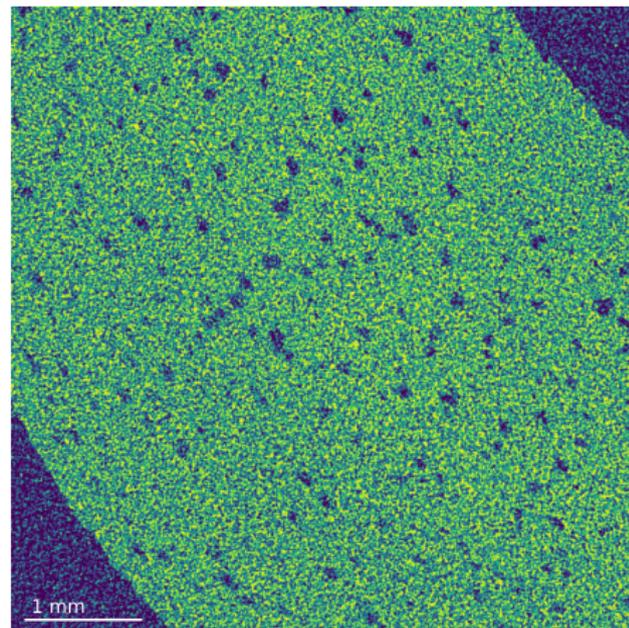
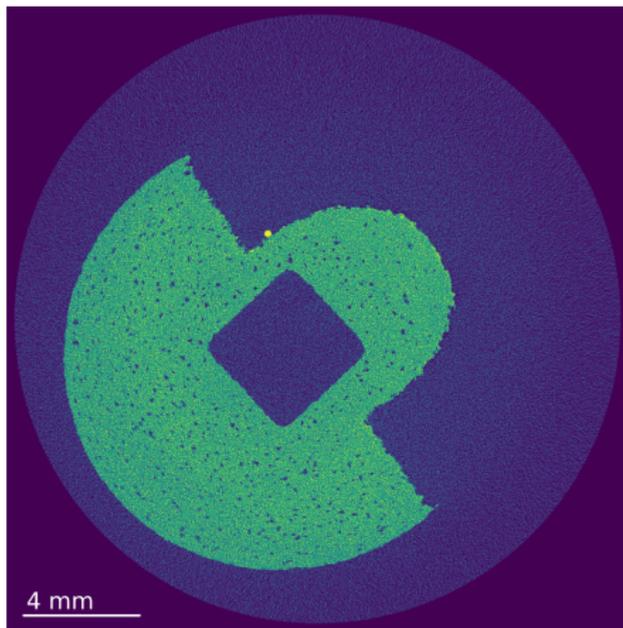


middle slice, LQ scan





$\frac{1}{4}$ slice, LQ scan



$\frac{1}{4}$ slice, LQ scan

Introduction, alignment in parallel tomography
example

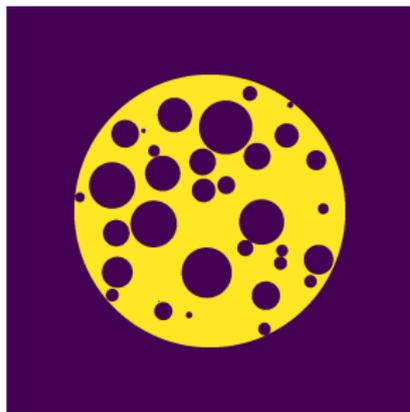
Fan-beam tomography
alignment via fixed point iteration

Cone-beam tomography
alignment via variable projection
on data
on real data

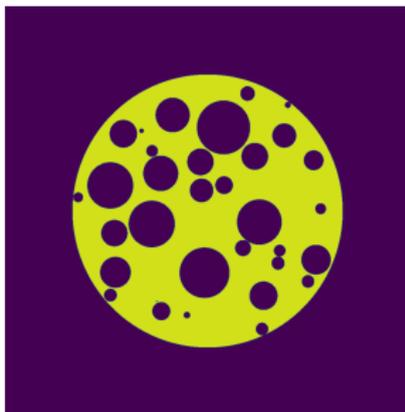
After alignment, regularized reconstruction

Conclusions and perspectives

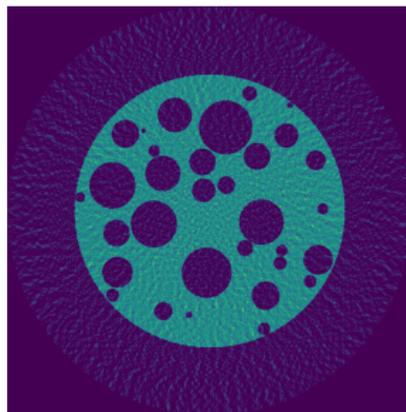
- Motivation: undersampled data



Phantom



FBP 1024 projections



FBP 60 projections

- Instead of FBP, we pose the problem as

$$\min_{u \in U} f(u) + g(Lu), \quad f, g \text{ convex}, \quad f \text{ smooth}, \quad L \text{ linear} \quad (\text{PP})$$

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- Recall the conjugate f^* of f

$$f^*(w) = \sup_{u \in U} \langle w, u \rangle - f(u)$$

then we have the dual problem of (PP)

$$\max_{w \in W} -g^*(-L^*w) - f^*(y) \quad (\text{DP})$$

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- Both (PP) and (DP) are solved e.g. with the Condat-Vu algorithm⁸:

$$\begin{cases} u_{k+1} = u_k - \tau \nabla f(u_k) - \tau L^* w_k \\ w_{k+1} = \text{prox}_{\sigma g^*}(w_k + \sigma L u_{k+1}) \end{cases}$$

⁸Condat. J. Optim. Theory Appl. 2013

- Total variation-regularized reconstruction:

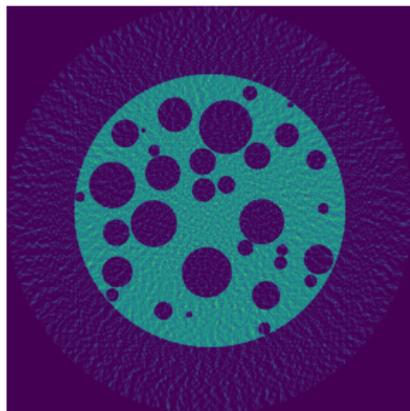
$$f(u) = \frac{1}{2} \|\mathcal{R}u - v\|_2^2, \quad g(w) = \lambda \|w\|_{2,1}, \quad L = \nabla,$$
$$\nabla f(u) = \mathcal{R}^*(\mathcal{R}u - v), \quad L^* = -\text{div}, \quad \text{prox}_{\sigma g^*}(w) = \Pi_{\|w\|_{2,\infty} \leq \lambda}$$

- Total variation-regularized reconstruction:

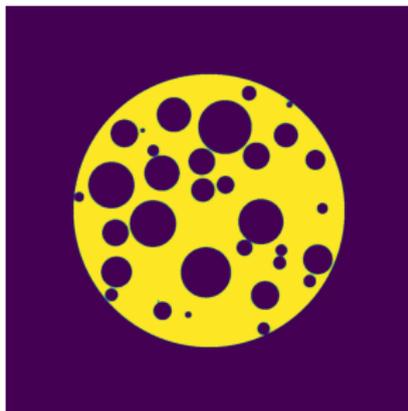
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- Ex: 60 noiseless projections



FBP

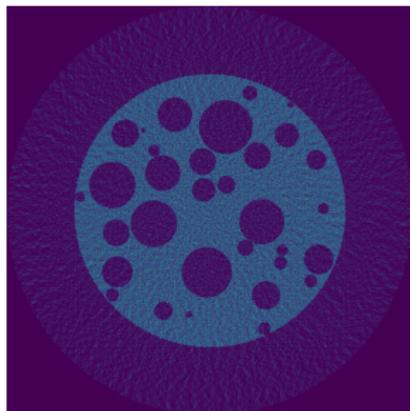


Condat-Vu

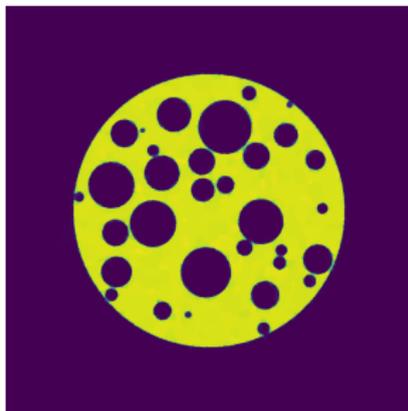
- Total variation-regularized reconstruction:

$$f(u) = \frac{1}{2} \|\mathcal{R}u - v\|_2^2, \quad g(w) = \lambda \|w\|_{2,1}, \quad L = \nabla,$$
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- Ex: 60 projections with Poisson noise



FBP



Condat-Vu

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on data
on real data

After alignment, regularized reconstruction

Conclusions and perspectives

- Goal: Fast, accurate and automatic tomography-based in-line industrial inspection
- Convergence analysis of different algorithms to design a new 'tomography-adapted' algorithm
- Resolution analysis needs to be done with different f, g, L
- \mathcal{R} and \mathcal{R}^* are expensive, we need faster approximations

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- Convergence analysis of different algorithms to design a new 'tomography-adapted' algorithm
- Resolution analysis needs to be done with different f, g, L
- \mathcal{R} and \mathcal{R}^* are expensive, we need faster approximations
- If challenging data, combine different regularizers by solving

$$\min_{u \in U} f(u) + g(Lu) + h(Ku), \quad f, g, h \text{ convex}, \quad L, K \text{ linear}$$

→ gracias !